





Finger-vein Image Enhancement and 2D CNN Recognition

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Finger vein recognition technology is a novel biometric technology with multiple features such as live capture, stability, difficulty in stealing and imitating, and more in the field of information security that has been utilized in a wide range of applications. In this proposed method, the finger region is separated from the background using a Sobel Edge detector and a Poly ROI which helps shape the finger. The background separation enhancement of low contrast using dual contrast limited adaptive histogram equalization which works on the visual characteristics of the finger-vein image dataset. When dual CLAHE is applied, the finger-vein histogram intensity is separated all across the image. Following the implementation of DCLAHE, an enhanced 2D-CNN model is utilized to recognize objects with the updated dataset. By maximizing the values of a preprocessed dataset, the 2D CNN model learns features. This model has a 94.88% accuracy rate.

Keywords: biometric; contrast limited adaptive histogram equalization; Sobel edge detector; poly region of interest and two dimensional convolution neural network.

INTRODUCTION

Personal identification is currently achieved using biometric technology used in a variety of security applications such as mobile phones, computer access, border crossing, banks, and ATMs. Fingerprint, iris, face, voice, and finger-vein recognition are some of the methods used (FV) [1, 2]. Because the vein patterns beneath the skin differ, the finger-vein recognition system has gotten a lot more attention in recent years. As a result, finger-vein recognition suggests a safe and practical technique for human biometric classification [3]. Traditional methods for recognizing finger veins rely on extracting lines from the input image or amplification and feature extraction [4]. Near-infrared (NIR) light is used to capture vein



images on the finger, and a charged coupled device (CCD) camera is used to record vein images beneath the finger [5]. Because the dataset needed to be normalized for the preprocessing step, the bitmap image was turned into a grayscale dataset with a single dimension for preprocessing and 2D CNN implementation [15]. When NIR penetrates the dorsal side of the finger and a CCD camera penetrates the palmar side, the region of the finger vein appears darker [6].

Finger vein datasets can be found in a variety of formats. The proposed approach for finger vein recognition was evaluated using the SDUMLA-HMT database [7]. Other finger vein datasets include HKPU-FV [8], UTFV [9], MMCBNU 6000 [10], THU-FV [11], and others. Local binary pattern (LBP) [12], Gabor filters (GF) [13], local derivative pattern (LDP) [12], and other techniques have been utilized to recover finger-vein images from the backdrop. Because these techniques have a weakness in similar settings such as translation and rotation during the capture of finger vein images, the deep learning technique known as convolutional neural network (CNN) is used for the classification of finger vein images. CNN/ConvNet is a deep learning algorithm that is faster than standard techniques [14].

Our suggested technique starts with a preprocessed Dual CLAHE [7] image dataset and feeds these preprocessed finger-vein images into a two-dimensional CNN model. Before classifying finger veins and applying enhancement techniques, our model uses a Sobel edge detector and a polygonal region of interest (ROI) to extract the background of the finger region [15]. As a result, we employ our image for histogram equalization follow extraction, which improves the image dataset. A histogram is a graphic representation of the distribution of greyscale values of pixels in a greyscale image [16]. The histogram's equalization distributes grey values uniformly throughout the image. Dual contrast limited adaptive histogram equalization (CLAHE) is used twice in the suggested technique to boost grey values in a finger vein image. Based on the folder names, the processed dual CLAHE finger vein images are classified. These pictures are then organized and utilized in the suggested 2D CNN model. In contrast to prior methods for extracting finger veins from picture datasets, 2D CNN algorithms can detect finger veins on a large scale of the dataset by learning features and recognizing them without removing background characteristics. According to the findings, 2D CNN is capable of locating finger veins with a high degree of accuracy.

The paper is organized as follows. The related study on finger-vein detecting technology is described in Section 2. Section 3 explains the finger-vein background extraction, Dual CLAHE, and 2D CNN architecture. The model's result and explanation are shown in section 4, and the conclusion is presented in section 5.

RELATED WORK

According to prior studies [1, 4], preprocessing and feature deduction approaches are commonly used in the detection of finger veins. The Gabor Filters have variable forms and directions to locate the finger-vein pattern [17]. The researcher utilized the local binary pattern (LBP) [18] and local derivative pattern (LDP) techniques to extract finger-vein patterns in [12]. The Gabor filter is used to match the SIFT features of vein patterns in the finger-vein classification [19, 20]. The principal component analysis (PCA) technique is used to create different traits [21]. Finger-vein feature extraction using sparse representation, the maximum curvature approach, HOG, and SVM are some of the documented strategies [23].



The algorithms for recognizing finger veins described above are standard. To improve the performance of finger-vein recognition, the researcher uses deep learning CNN-based algorithms instead of standard approaches [1]. In [24], the author developed a CNN technique for finger recognition that combines a reduced-complexity four-layer with fused convolutional-subsampling. In [24] suggested a CNN approach that consists of seven layers, five of which are convolutional layers and two of which are fully connected layers. The challenge of irregular size for features is acceptable resolved with a PCA-based dimensionality reduction strategy in the [26] paper, which employs a method that uses a multimodal finger fusion based on CNN. These procedures, on the other hand, are either more difficult or incapable of delivering the required results. On the other extreme, these treatments are either more complex or incapable of producing the desired effects.

THE PROPOSED METHOD

Overview. In this study, finger-vein recognition is broken down into six steps, as shown in the flow diagram in Figure 1. The SDUMLA-HMT picture database [7], which is a free collection of finger-vein images, is used to read the first photos. As observed in Figure 2(a) and Figure 2(b), the finger-vein images in the dataset are standardized, which is normalized in the second phase, which changes the image dataset into greyscale images of size, as seen in Figure 2(a) and Figure 2(b). The third step is to extract our backdrop from the finger-vein pictures dataset (see Figure 2(c)). The Sobel edge detector and polygonal ROI are used to obtain the finger region. The finger-vein picture dataset is first run through the dual CLAHE, which produces dark vein ridges, before being fed into the 2D CNN deep learning model. The architecture of the 2D CNN with twenty layers, as shown in Figure 9, is shown below.

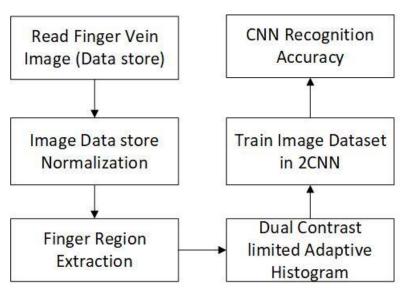


Figure 1. The proposed method's flow diagram.

Sobel Edge Detector and Poly ROI.

At the points where the gradient is the highest, it appears ahead of the edges. By performing a 2-D spatial gradient quantity on a picture, the Sobel method accentuates regions of high spatial frequency that correlate to edges. It only takes the finger boundary of the finger-



vein image [31]. So after the Sobel edge detector detects some areas of the finger and detects some of the backgrounds at the corner of the image, it cannot discriminate the finger region, so for this, it uses polygonal ROI to shape the finger part. Polygonal ROI creates a binary mask for the finger region to subtract the finger from the background portion and take the finger to detect finger-vein edges [32]. Figure 2(c) illustrates the result of separating the finger region from the background part.

Dual CLAHE. Considering that the contrast of the dataset's finger-vein images is too low, the finger-vein cannot be distinguished from the background or skin region, we utilized a dual CLAHE enhancement technique [7], in which it is applied twice to the finger-vein image. The finger-vein image is cropped and reduced using this technique from the black region, which is the background portion of the original image that has been removed. We used dual CLAHE to enhance the vein region twice after cropping the finger-vein image, as shown in Figure 3. CLAHE is a modified form of Adaptive Histogram Equalization (AHE) that works on small parts of the contextual region [28] in the finger-vein picture known as tiles 22 on both CLAHE and AHE. CLAHE with the same exponential distribution [7], [27], with clipping limits of 0.03 on the first and 0.04 on the second.

$$N_{avg} = \frac{N_r X \times N_r Y}{N_{gray}} \tag{1}$$

The average number of pixels is represented by N_{avg} , the number of gray-scale pixels is represented by N_{gray} , and pixel amounts in the X and Y directions are represented by N_rX and N_rY , respectively, as indicated in Eq. (1).

The CL (clipped limit) is a value that is limited to a specific threshold where grayscale is darker and is considered finger-vein as follows:

$$N_{CL} = N_{clip} \times N_{avg} \tag{2}$$

$$N_{\text{avggray}} = \frac{N_{\text{Eclip}}}{N_{\text{gray}}} \tag{3}$$

Within the range of the [0 1] array, the actual CL is N_{clip} , where the real CL is N_{CL} . Only when it exceeds the pixel number N_{CL} is it clipped. $N_{\Sigma clip}$ is the total number of pixels clipped, and the remaining average grey-level pixels are distributed as in Eq. (3) [7], [27].



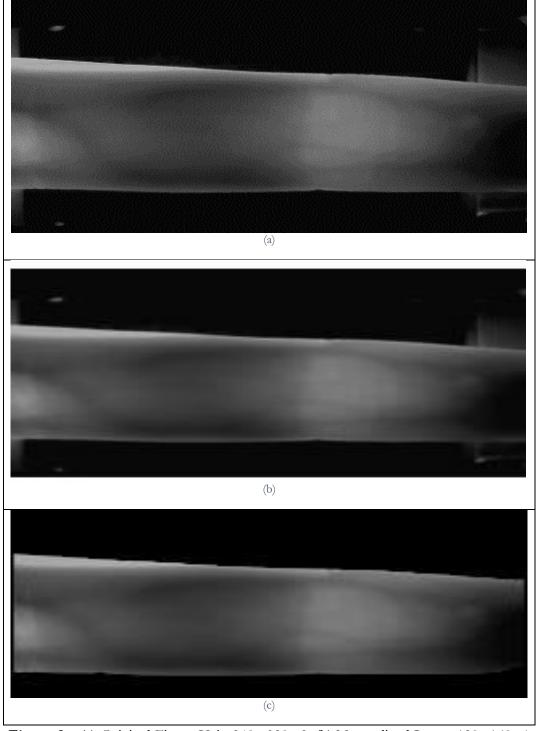


Figure 2. (a) Original Finger Vein 240×320×3, (b) Normalized Image 120×160×1, (c) Finger Region Extraction using Sobel edge detector and polygonal ROI.





Figure 3. Dual CLAHE implementation.

2D CNN Network Architecture. The image input layer has a size of pixels, and there are four 2D convolutional layers, four batch normalization layers, and four rectified linear units (ReLU) with three max-pooling layers, two fully connected layers, one softmax layer, and a classification output layer. Learning characteristics from finger veins is 94.38% accurate. The convolutional layer concatenates different sizes of filters on the finger-vein image dataset to learn features of the finger-vein image for the image recognition system, as demonstrated in Figure 4 which shows the initial convolutional layers. The first convolutional layer employs five filters and [2 2 2 2] padding to maintain the image size by adding two zeros to the top, bottom, left, and right of the finger-vein image matrix. Ten, twenty, and thirty filters of various sizes are used in the convolutional layers, as shown in Figure 9.

$$y = \sum_{c=1}^{N} w_c * x_c + b \tag{4}$$

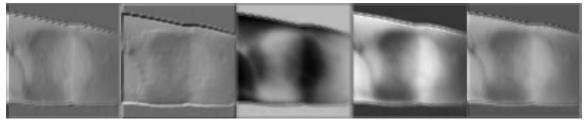


Figure 4. First Convolution Output Layer.

 ω_c is the weight array of a 2D filter in the c^{th} input channel, x_c is the 2D input of the c^{th} channel filter, and b is the bias of a filter in the above Eq. (4). As seen in Figure 5, batch normalization substitutes this bias with a β -shift factor. The sizes of channels may fluctuate with the bias factor after convolving the finger-vein input images with different filters, hence batch normalization normalizes the channels for ReLU activation [28].

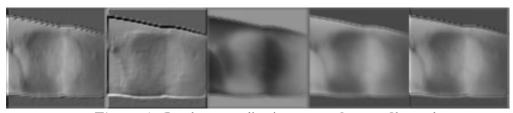


Figure 5. Batch Normalization Layer Output Channels.



The ReLU layer, as shown in Figure 6 [5], is an activation function that increases nonlinearity after batch normalization. ReLU employs the maximum pixel value in this model. Pixels less than zero are referred to as 0, whereas pixels larger than zero are referred to as y. Non-linear functions such as tanh and sigmoid were previously employed. Eq. (5) [1], [5] shows how the researcher determines the ReLU:

$$f(y) = \max(0, y) \tag{5}$$



Figure 6. ReLU Layer Output Channels.

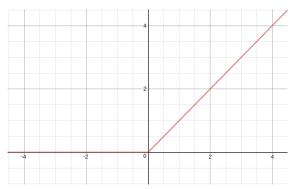


Figure 7. Graph of ReLU Layer.

The max-pooling layer with a filter matrix will take the maximum values, taking only the maximum number of channel values. The stride of the max-pooling layer is [2 2] with padding. The maximum pooling output is shown in Figure 7.

We apply this function of the fully connected layer two times $t = f_c(x, \omega, b)$, where x represents the input of this layer, w represents the weight matrix, b represents the bias, and t represents the output [29], which is as described in Eq. (6):

$$t_{i'} = \sum_{i} w_{ii'} x_i + b_i \tag{6}$$

For each image location used to classify pixels into one of the initial labels where the linked object classes belong, the second final layer of 2D CNN generates a probability



distribution. For multi-elegance category issues, the category output layer employs the passentropy lack of reciprocally absolute instruction [30].

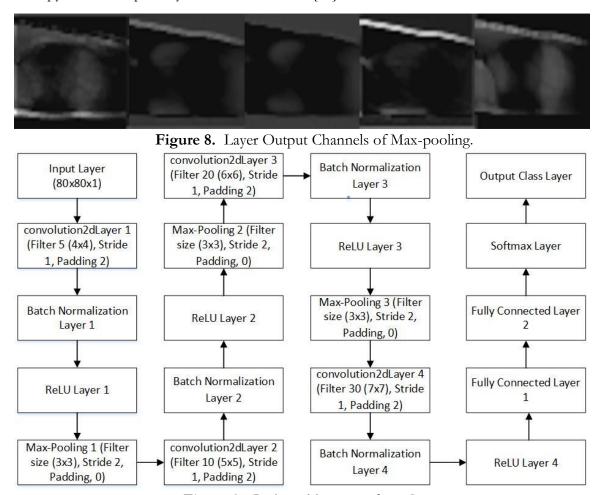


Figure 9. Basic architecture of 2D CNN.

RESULT

The preprocessed dataset of the dual CLAHE finger-vein picture dataset is randomly divided into 80 percent training, 20 percent validation, and 20 percent test images, with four index, middle, and ring finger classes in each folder. These divided data are fed into an Adam optimizer-based train network, which optimizes the learned values from our CNN model and detects features in each image. In this version, we extract four preprocessed finger-vein pictures from each folder of the left and proper hands, labeling them with the names of the index, center, and ring palms. The training option employs an Adam optimizer with a maximum epoch of 80, with one epoch equaling one complete cycle and twelve iterations. The training progress report in Figure 10 shows that after 960 iterations, the validation accuracy for learning the dual CLAHE preprocessed image dataset with various classes is 94.88 %.



The Adam optimizer is used to train the 2D CNN model and update network weights. The epoch values, iteration, iteration per epoch, and validation frequency are shown in table (1) below. Figure 11 depicts a model loss in which the weight may be replenished and the loss reduced on subsequent review. The blue line in Figure 10 depicts the training (smoothed), which is less noisy. The light blue line represents training, which classifies individual minibatches, while dotted or dashed lines indicate validation, which classifies the complete collection. In Figure 10, the blue line illustrates the training (smoothed), which is less noisy. The light blue line is the training that classifies individual mini-batches, and validation is represented by dotted or dashed lines that classify the entire set. The training loss on each mini-batch is shown in Figure 11 in light orange, the smoothed training loss in orange, and the validation loss in dotted or dashed lines.

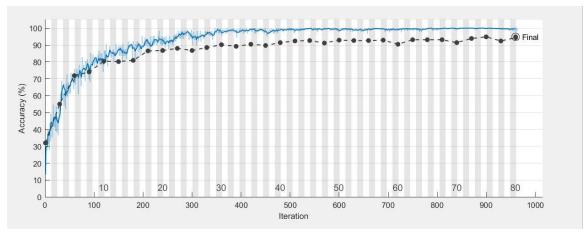


Figure 10. 2D CNN accuracy graph.

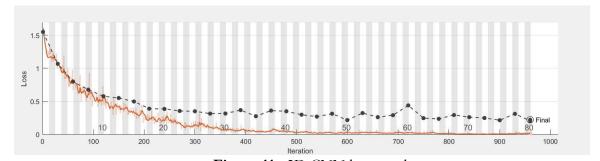


Figure 11. 2D CNN loss graph. **Table 1.** Table describing sample of IJIST.....

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#	Parameter	Values
1	Validation accuracy	94.87%
2	Epoch	80
3	Iteration	960
4	Iteration per epoch	12



5 Validation Frequency

30 iteration

CONCLUSION

In this research work, we used 2544 images to separate the finger region from the background using a Sobel edge detector and poly ROI, which shaped the acquired edges of the finger and created a binary mask to separate out the finger. The finger-vein dataset is enhanced using dual CLAHE and after enhancing the finger-vein images, these datasets are further utilized in 2D CNN where the model learns the features of every segmented finger-vein. The finger-vein images are divided into distinct classes of folders such as index, middle, and ring folders, with 2D CNN taking four images from each folder. Hence, our version became capable of examining the traits of every photo as well as distinguishing every photograph inside folders. The suggested model's accuracy is 94.88%.

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Author's Contribution. Noroz Khan is the author and conducted this research under the supervision of Saleem Ahmed. Ramesh Kumar, the co-supervisor.

Conflict of interest. There is no conflict of interest declared by the authors.

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